

Redox modulated hydrogelation of a self-assembling short peptide amphiphile

CAO ChangHai¹, CAO MeiWen¹, FAN HaiMing¹, XIA DaoHong¹, XU Hai^{1*} & LU Jian R^{2*}

¹The Centre for Bioengineering and Biotechnology, China University of Petroleum (East China), Qingdao 266580, China;

²Biological Physics Group, School of Physics and Astronomy, University of Manchester, Manchester M13 9JP, United Kingdom

Received May 12, 2012; accepted August 29, 2012; published online September 25, 2012

Hydrogels resulting from the self-assembly of small peptides are smart nanobiomaterials as their nanostructuring can be readily tuned by environmental stimuli such as pH, ionic strength and temperature, thereby favoring their practical applications. This work reports experimental observations of formation of peptide hydrogels in response to the redox environment. Ac-I₃K-NH₂ is a short peptide amphiphile that readily self-assembles into long nanofibers and its gel formation occurs at concentrations of about 10 mmol/L. Introduction of a Cys residue into the hydrophilic region leads to a new molecule, Ac-I₃CGK-NH₂, that enables the formation of disulfide bonds between self-assembled nanofibers, thus favoring cross-linking and promoting hydrogel formation. Under oxidative environment, Ac-I₃CGK-NH₂ formed hydrogels at much lower concentrations (even at 0.5 mmol/L). Furthermore, the strength of the hydrogels could be easily tuned by switching between oxidative and reductive conditions and time. However, AFM, TEM, and CD measurements revealed little morphological and structural changes at molecular and nano dimensions, showing no apparent influence arising from the disulfide bond formation.

peptide amphiphiles, self-assembly, hydrogelation, redox stimuli

Citation: Cao C H, Cao M W, Fan H M, et al. Redox modulated hydrogelation of a self-assembling short peptide amphiphile. *Chin Sci Bull*, 2012, 57: 4296–4303, doi: 10.1007/s11434-012-5487-2

Peptide hydrogels have been actively exploited for a variety of biomedical applications such as cell culture, regenerative medicine, controlled drug and gene delivery [1–15]. Most peptide hydrogels arise from the entanglement of self-assembled nanoobjects such as nanofibers and nanotubes. Peptide self-assembly is driven by the orchestrated interaction of several intermolecular non-covalent forces including hydrogen bonding, π - π stacking, hydrophobic effect and electrostatic interactions. Environmental stimuli including pH [16–19], ionic strength and/or metal ions [18,20–22], temperature [23], light [24] and enzyme-triggers [25], provide powerful approaches for modulating hydrogelation. Furthermore, introduction of microenvironment-sensitive amino acid residues into peptide sequences is also an important strategy for controlling peptide self-assembly and hydrogelation [9,26–28].

Most of the self-assembling peptides, capable of forming nanofiber hydrogels, either carry more than 10 amino acid residues or contain non-amino acid moieties such as 9-fluorenylmethoxycarbonyl and long alkyl groups, which favor the self-assembly and hydrogelation through aromatic stacking and/or hydrophobic interaction. In a recent study, we have designed an ultrashort peptide amphiphile Ac-I₃K-NH₂, consisting of three consecutive hydrophobic Ile residues and a charged Lys residue, and found that it could readily self-assemble into long nanofibers in aqueous solution [29]. These nanofibers could entangle to form a network, thus reducing the fluidity of solution and finally resulting in hydrogelation at a concentration of 10 mmol/L (0.53%, w/v). However, rheological measurements indicated that these I₃K hydrogels were not very stiff, with storage moduli being some 200–300 Pa at the frequency range of 0.1–10 Hz. Enhancement or modulation of mechanical properties of hydrogels always favors their practical

*Corresponding authors (email: xuh@upc.edu.cn; j.lu@manchester.ac.uk)

applications. In this work, the Cys residue has been introduced into the Ac-I₃K-NH₂ sequence at the interface of hydrophobic/hydrophilic residues. Thiol groups can couple to form disulfide bonds which may improve the gelling property [18]. Furthermore, the covalent crosslinking can occur in benign conditions (i.e. air oxidation) without additional chemical agents, which is helpful in preserving the biocompatibility and biodegradability of the system concerned. Additionally, a Gly residue was inserted between Cys and Lys in order to create more space for disulfide bond formation, giving the final target sequence of Ac-I₃CGK-NH₂. For comparison, we have also designed another peptide, Ac-I₃MGK-NH₂, where the thiol group is methylated, thus preventing disulfide bond formation. The chemical structures and space-filling models of the designed peptides are shown in Figure 1.

1 Materials and methods

1.1 Materials

Protected *L*-amino acids (Fmoc-Ile-OH, Fmoc-Cys(Trt)-OH, Fmoc-Gly-OH, Fmoc-Met-OH and Fmoc-Lys(Boc)-OH), O-Benzotriazole-*N,N,N',N'*-tetramethyluronium hexafluorophosphate (HBTU), *N*-hydroxybenzotriazole (HOBT), *N,N*-diisopropyl ethylamine (DIEA), Trifluoroacetic acid (TFA), Trisopropylsilane (Tis) and MBHA resin were purchased from GL Biochem (Shanghai) Ltd. and used as received. Piperidine, dichloromethane (DCM) and *N,N*-dimethyl formamide (DMF) were purchased from Bo Maijie Technology, and were redistilled prior to use. Other reagents were obtained from Sigma and used without further purification. Milli-Q water (18 MΩ cm) was used for all the

experiments.

1.2 Peptide synthesis

The peptides were synthesized using the Fmoc solid-phase synthesis strategy from natural *L*-amino acids, on a CEM Liberty microwave peptide synthesizer. As shown in Figure 1, the N- and C-termini of the peptides were acetylated and amidated, respectively, to eliminate the effect of terminal charges that are believed to complicate the process of self-assembly. The detailed procedures have been described in our previous work [30–33]. Deprotection, activation, coupling and capping were carried out on the synthesizer and cleavage from the resin was finished manually away from the synthesizer. The cleavage mixture was then filtered into a round-bottomed flask and evaporated to a concentrated solution which was subsequently dropped into cold ether for precipitation. The ether solution was centrifuged at 4°C and 7000 r/min for 10 min and the solid product was collected. The cold ether precipitation procedure was repeated at least six times and the finally collected product was lyophilized for 2 d. Note that the Ac-I₃CGK-NH₂ sample was stored in N₂ atmosphere after lyophilization. MALDI-TOF (matrix assisted laser desorption ionization time-of-flight) and reverse-phase HPLC analysis indicated the higher purity (>90%) of the final products (see Figures S1 and S2 in the Supporting Information for spectra).

1.3 Sample preparation

An appropriate amount of peptide was dissolved in air-free Milli-Q water at the desired concentration giving a final pH of 5–6. After quickly dissolving Ac-I₃CGK-NH₂, 1.0 mL of

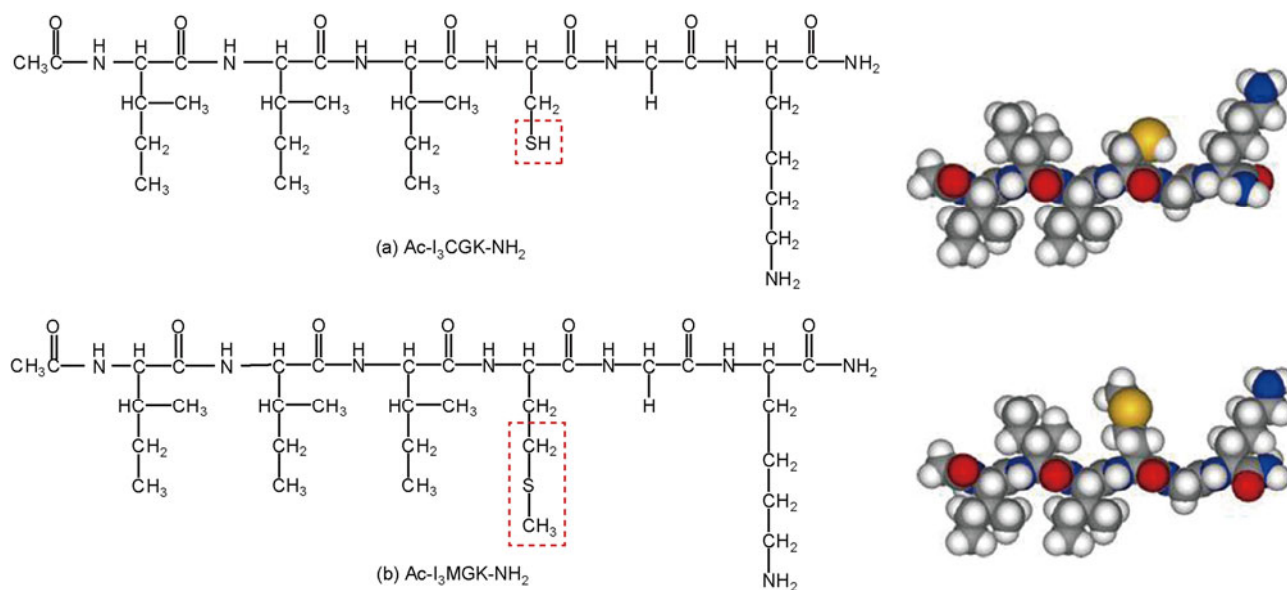


Figure 1 Chemical structures and space-filling models of (a) Ac-I₃CGK-NH₂ and (b) Ac-I₃MGK-NH₂. The red dashed lines highlight the structural differences between the two peptides. Color scheme: carbon (black), hydrogen (white), oxygen (red), nitrogen (blue), and sulfur (yellow).

the peptide solution was immediately transferred into 8 mL glass vials (the vial's diameter is 2.0 cm), which were then tightly sealed. Thus the upper air space provided the oxygen source for the Cys oxidation. The oxidation time was counted after peptide dissolution. Note that during the oxidation process, no shaking or stirring was performed.

1.4 Circular dichroism (CD)

CD spectra were recorded on a Biologic Mos-450/AF-CD spectrophotometer at room temperature using a 0.1 mm quartz cell. Scans were collected between 190 and 260 nm in steps of 0.5 nm, with an acquisition time of 2 s. These spectra were averaged and smoothed to improve the signal-to-noise ratio using the software (Bio-kine 32 V 4.49) supplied by the vendor. The results are here expressed in Millidegree.

1.5 Attenuated total reflectance-Fourier transform infrared spectroscopy (ATR-FTIR)

ATR-FTIR of the peptide solution (1.71 mmol/L in D₂O to avoid interference by H₂O which exhibits strong adsorption near 1640 cm⁻¹) was collected at a Nicolet 6700 FT-IR spectrometer equipped with a DTGS detector. An ARK HATR accessory equipped (Thermal Electron) with a ZnSe crystal and a trough sampling plate was used. The spectra were recorded at room temperature, and 256 scans were measured with a spectral resolution of 4 cm⁻¹ to obtain a good signal-to-noise ratio. Using the OMNIC software package, background and solvent spectra were subtracted and the spectra were smoothed.

1.6 Rheology

Rheological measurements were performed on a Physica MCR 301 rheometer (Anton Paar) operating in cone-plate mode (cone angle 1.007° with diameter of 49.959 mm). Peptide samples were transferred to the rheometer stage. After equilibration, dynamic frequency sweep (0.1–10 Hz and 0.1% strain) and dynamic strain sweep (1 Hz and 0.01%–100% strain) experiments were performed at 25°C.

1.7 Atomic force microscopy (AFM)

AFM measurements were performed with a commercial Nanoscope IVa MultiMode AFM (Digital Instruments, Santa Barbara, CA) in tapping mode at room temperature. For ambient AFM imaging, 10 µL of peptide solution was deposited onto a freshly cleaved piece of mica. After 2 min, the sample was dried with a gentle stream of nitrogen. Probes used are RTESP silicon probe (Veeco, Santa Barbara, CA) having a typical tip radius of ~10 nm, attached to 125 µm cantilevers with a nominal spring constant of 42 N/m. All images were acquired with a scan speed of 1.0–1.5

Hz and at a scan angle of 0°, and flattened using a first-order line fit to correct for piezo-derived differences between scan lines. In each case, topographic and phase images were recorded concurrently, and scans were made at least three times. Representative images are shown here.

1.8 Transmission electron microscopy (TEM)

TEM sample preparation was done from peptide solutions using negative-staining. A drop of peptide solution was placed on a 400 mesh copper grid covered by carbon-stabilized Formvar film. After 5 min, excess liquid was sucked away by filter paper and the grid was negatively stained with 2% uranyl acetate aqueous solution. The samples were imaged under a JEOL 1200EX electron microscope operated at 200 kV.

1.9 Ellman test

The Ellman test was used to determine the amount of thiol groups and is known to work well for small peptide and proteins synthesized through standard solid phase synthetic methods [34]. First, 5,5'-dithio-bis(2-nitrobenzoic acid) (DTNB) stock solution (50 mmol/L sodium acetate, 2 mmol/L DTNB in H₂O) and Tris buffer solution (1 mol/L, pH 8.0) were prepared and refrigerated. To obtain the calibration curve, the standard H-Cys-OH·HCl solutions were prepared from 0.1 mmol/L to 2.0 mmol/L. Then 50 µL of DTNB solution, 100 µL of Tris solution and 840 µL of water were put into a cuvette and mixed carefully using a pipette to get the DTNB reagent (990 µL), which was scanned by UV spectrophotometer (1700 Pharma Spec, Shimadzu) at 412 nm to obtain the background spectrum. Then 10 µL of H-Cys-OH·HCl solution (or the standard solutions) was added into the 990 µL DTNB reagent, stirred and incubated for 5 min at room temperature. The solution absorbance at 412 nm was recorded twice. The calibration curve was obtained by plotting the absorbance value of each H-Cys-OH·HCl solution as a function of concentration (see Figure S3). For the determination of thiol groups in the Ac-I₃CGK-NH₂ solution, the same procedure was performed and the thiol concentration was calculated by referring the observed absorbance value at 412 nm to the calibration curve. Note that because each Ac-I₃CGK-NH₂ molecule carries one thiol group, the determined thiol concentration should be equal to the concentration of Ac-I₃CGK-NH₂.

2 Results and discussion

Ac-I₃K-NH₂ molecules self-assembled in aqueous solution to form long nanofibers that tended to entangle with increasing peptide concentration [29]. At a relatively high concentration of 10 mmol/L, a self-supporting gel formed, but possessed weak mechanical properties with the storage

modulus (G') being 200–300 Pa. At lower concentrations typically below 4 mmol/L, peptide solutions were always freely flowing liquids, regardless of incubation time. Upon introduction of a Cys residue, however, Ac-I₃CGK-NH₂ was found to form a self-supporting hydrogel even at a low concentration of 0.5 mmol/L after some 40 d of incubation (Figure 2). The hydrogel, formed at the concentration of 1.71 mmol/L and after 6 d of incubation, displayed significantly enhanced mechanical properties, with G' values of ~4500 Pa (Figure 3(a)). Also note that G' and G'' (loss

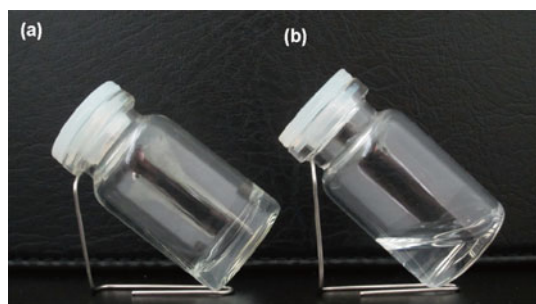


Figure 2 Photographs of (a) 0.5 mmol/L Ac-I₃CGK-NH₂ and (b) 0.5 mmol/L Ac-I₃K-NH₂ after 40 d of incubation in air.

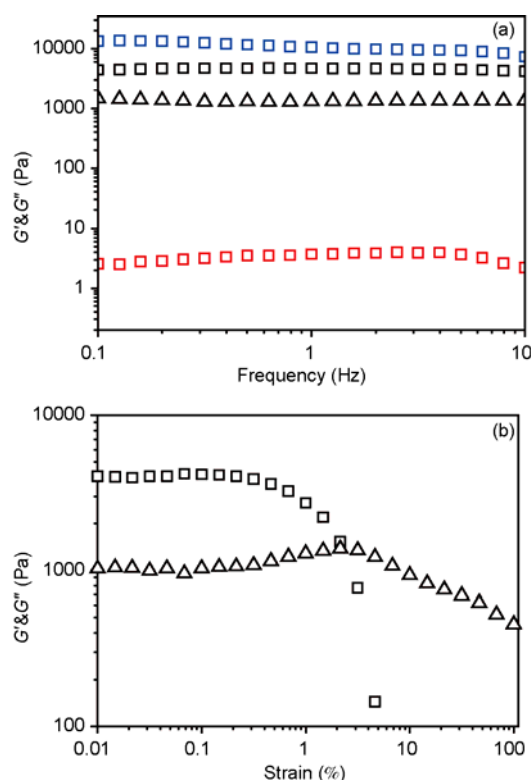


Figure 3 Oscillatory rheological measurements of 1.71 mmol/L peptide solutions after 6 d of incubation at different environmental conditions. Storage modulus (G' , square) and loss modulus (G'' , triangle) measured with (a) frequency sweeps from 0.1–10 Hz with 0.1% constant strain and (b) Strain sweep from 0.01% to 100% strain at 1 Hz oscillation at 25°C. Color scheme: Ac-I₃CGK-NH₂ (black), Ac-I₃CGK-NH₂ with H₂O₂ (blue), and Ac-I₃CGK-NH₂ with DTT (red). Note that the G'' values with H₂O₂ and DTT are not shown here for clarity.

modulus) were frequency insensitive in this frequency range. The vast increase in G' and G'' might arise from the cross-linking of peptide nanofibers through disulfide bond formation. Figure 3(b) shows G' and G'' against strain for the same gel at a 1 Hz oscillation. Little variation in G' and G'' was observed up to a strain of approximately 1%. A linear viscoelastic regime could thus be ensured for the frequency sweep experiments at a constant strain of 0.1%. Additionally, further increase in peptide concentration shortened gelation time.

To verify this hypothesis, we first examined the effect of addition of reducing agent DTT as it can prevent disulfide bond formation. DTT was added to the aqueous solution immediately after dissolving the peptide at an Ac-I₃CGK-NH₂/DTT molar ratio of 1:3. After 6 d of incubation, the 1.71 mmol/L peptide solution containing DTT remained in a free liquid state, and its G' values were consistently low (less than 10 Pa), which were about 3 orders of magnitude smaller than the values obtained from the system without DTT (Figure 3(a)).

To test the effect of oxidative agent, H₂O₂ was used as it exists widely in biological processes. In the first instance, the peptide solution of 1.71 mmol/L was incubated for 4 d to ensure the formation of protofibrils, followed by the addition of H₂O₂ with an Ac-I₃CGK-NH₂/H₂O₂ molar ratio of 1:5. On the 6th day, the peptide solution with H₂O₂ had G' values of ~10000 Pa, an increase by over a factor of 2 over the system without the peroxide (Figure 3(a)). When we substituted DTT for H₂O₂ in this process, the peptide solution on the 6th day exhibited G' values of ~180 Pa, showing that the clear effect of reduction of the disulphide bonds by DTT as a reducing agent.

Subsequently, we also examined the self-assembly and gelation process by the same amount of H₂O₂ added right at the beginning of peptide solution preparation. In this case, the peptide was oxidized to dimers. The self-assembled nanostructures were comprised of spherical stacks and short nanofibers (see Figure S4). The peptide solution did not show any gel-like response, suggesting a distinctly different self-assembling pathway.

The thiol concentration of the peptide solution was monitored using Ellman reagent. Air oxidation is one of the mildest approaches to construct a disulfide bond but usually requires long reaction time [35]. Consistent with this, the thiol concentration decreased gradually over time in the peptide solution in the absence of additional oxidative or reductive agent, as indicated in Figure 4(b). After 6 d of air incubation, the thiol concentration was reduced from some 1.71 mmol/L to 0.92 mmol/L, indicating ~46% oxidation, and after 40 d there was still ~10% non-oxidized. As indicated by the inset in Figure 4(b), however, the quantity of thiol groups decreased dramatically upon addition of H₂O₂ after 4 d of incubation. In fact, after 6 h of H₂O₂ addition there were few non-oxidized monomers.

Because air oxidation reaction takes place slowly, the

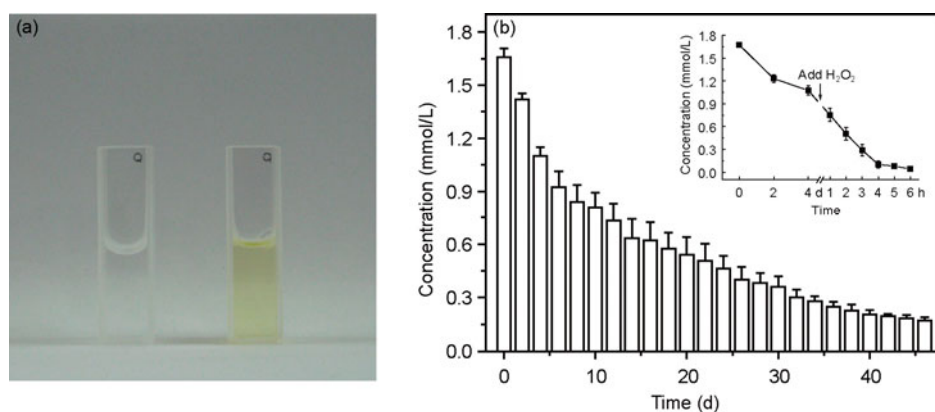


Figure 4 Standard “Ellman Test” for quantitative determination of thiol groups. The original peptide solution was prepared at a concentration of 1.71 mmol/L. (a) In the presence of thiol groups, colorless DTNB was transformed into yellow 2-nitro-5-thiobenzoic acid (TNB); (b) variation of the Ac-I₃CGK-NH₂ or thiol group concentration over time. The inset shows the decrease in the quantity of thiol groups after addition of H₂O₂.

viscoelastic properties of the Ac-I₃CGK-NH₂ gel can be tuned through oxidation time. Prolonging incubation time in air is expected to increase the gel's stiffness. The G' values were found to increase to ~15000 Pa after 25 d of incubation. There was 24% non-oxidized monomer at this time point. Besides, the more cross-linking of nanofibers resulting from increased disulfide bond formation, the further physical entanglement of nanofibers with time, leading to the significant improvement in the mechanical strength. On the other hand, because no additional chemicals were needed for air oxidation reaction and the process occurred spontaneously in aqueous solution, the resulting gel would be advantageous for various biomedical applications.

AFM and TEM were utilized to visualize the hydrogel nanostructures (Figure 5). Similar to Ac-I₃K-NH₂, Ac-I₃CGK-NH₂ also self-assembled into long nanofibers, in sharp contrast to the spherical nanostacks and short nanofibers formed from the oxidized peptide dimers if strong oxidant such as H₂O₂ is added right at the beginning of peptide solution preparation. Upon formation of peptide nanofibers, the hydrophilic CGK region is exposed to the outer surface. Subsequent disulfide bond formation helps to

crosslink already formed nanofibers into gel network. Thus, such chemical bond connections between the surfaces of nanofibers do not disrupt the morphology of the assembled fibers but instead, increase the connectivity of the nanofiber network (Figure 5).

To evaluate the secondary structures of the peptide assemblies in aqueous solution, CD measurements were first performed from the 1.71 mmol/L peptide solution and the result is shown in Figure 6(a). The positive band at 195 nm and negative band at 220 nm suggest a typical β -sheet structure. The two bands intensified dramatically over the first few hours. The β -sheet content, as indicated by the negative band at 220 nm, tended to equilibration after about 7 h (the inset of Figure 6(a)). This observation suggested that the protofibrils formed during this period, consistent with the AFM characterization (see Figure S5). The subsequent association and elongation of protofibrils to long and mature nanofibers did not alter the β -sheet structure. Also, the disulfide bond formation between nanofibers did not affect the secondary structure either. No secondary structural variation was observed after adding H₂O₂ into the system, showing that the promotion of disulfide bond formation

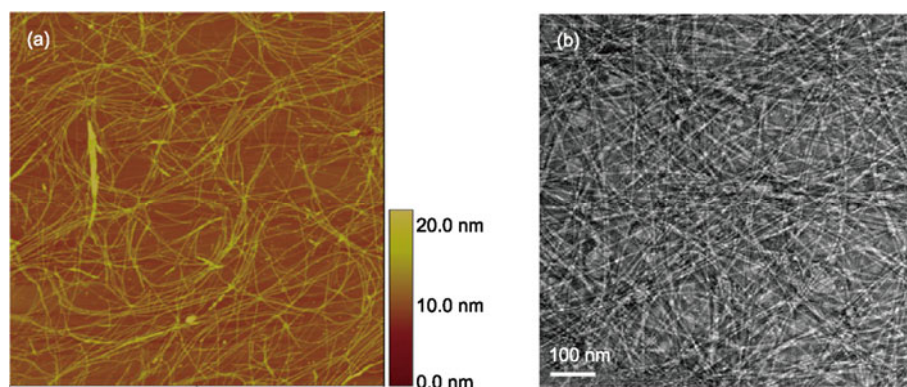


Figure 5 (a) AFM (5 $\mu\text{m} \times 5 \mu\text{m}$) and (b) TEM images of an Ac-I₃CGK-NH₂ hydrogel formed at the concentration of 1.71 mmol/L after 25 d of incubation in air. The height scale for the AFM image is 20 nm as indicated.

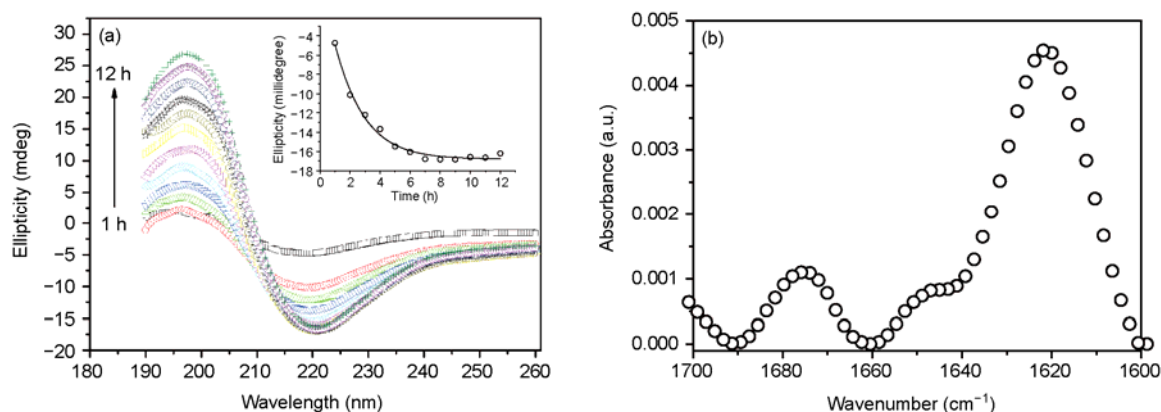


Figure 6 (a) Time-dependent CD spectra of 1.71 mmol/L Ac-I₃CGK-NH₂ in air. The inset shows ellipticity at 220 nm as a function of time. (b) FTIR spectrum (the amide I region) of 1.71 mmol/L Ac-I₃CGK-NH₂ solution in D₂O (2 d of incubation in air). All the spectra were obtained at room temperature.

between the nanofibers did not cause detectable changes to the β -sheet structure (data not shown). Furthermore, complementary FTIR characterizations in D₂O also indicated the predominance of β -sheet conformation (Figure 6(b)), where the two peaks centering at 1621 and 1675 cm⁻¹ are indicative of intermolecular anti-parallel β -sheet structure [36–39].

To further confirm the role of the Cys residue in the hydrogelation and the effect of disulfide bond formation, we designed Ac-I₃MGK-NH₂ in which disulfide bond formation was blocked by methylation. As shown in Figure 7, Ac-I₃MGK-NH₂ assembled into nanofibers and adopted predominantly a β -sheet structure, but did not form a gel at 1.71 mmol/L even after 60 d of incubation. The poor solubility of Ac-I₃MGK-NH₂ prevented us from evaluating its gelling potential over higher concentrations.

Figure 8 shows a schematic illustration for the Ac-I₃CGK-NH₂ gel formation. The peptide molecules firstly assembled into protofibrils by adopting a β -sheet structure, followed by elongation (end to end) and association (lateral) to long and thick fibers. The Cys residues distributed on the outer surface of the nanofibers are oxidized to disulfide

bonds, thus leading to significantly more crosslinking of the nanofibers. This chemical crosslinking, together with physical crosslinking with time, strengthens the interaction between fibers and results in the gelation at much lower concentrations. By controlling oxidation condition, the gelation kinetics and the mechanical properties of Ac-I₃CGK-NH₂ gels can be tuned in a facile way.

3 Conclusions

Ac-I₃K-NH₂ has been taken as a model sequence into which a Cys residue was introduced in order to demonstrate that incorporation of a chemical crosslinker in the form of the disulfide bond gives a means for controlling gel formation. This work has demonstrated that this facile approach can be generally applied to short self-assembling peptide systems. Redox conditions can be used as a means of controlling the rate and the occurrence of gelation. The realization of this control in hydrogel formation via disulfide bond crosslinking can be used to apply self-assembling peptides in a broad range of biomaterial and biomedical research.

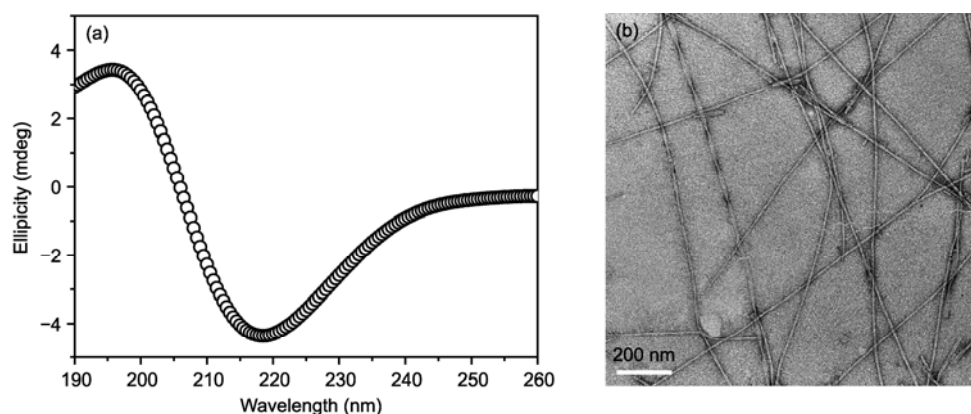


Figure 7 (a) CD spectrum and (b) TEM image of Ac-I₃MGK-NH₂ solution at 1.71 mmol/L.

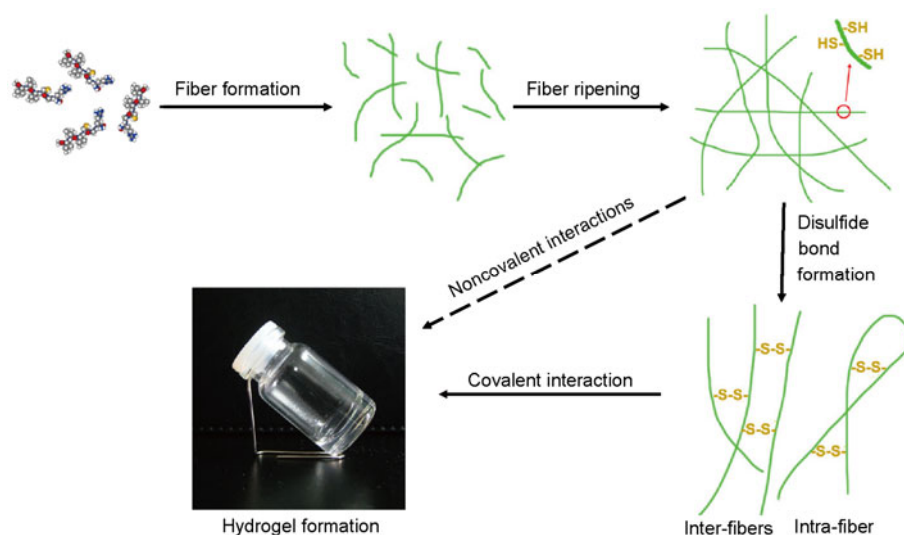


Figure 8 Schematic representation of gel formation. The covalent cross-link between cysteines can form intra- and inter-fiber disulfide bonds, which may function cooperatively with other noncovalent interactions to result in gel formation.

This work was supported by the National Natural Science Foundation of China (21033005, 21003160), the Natural Science Foundation of Shandong Province of China (ZR2010BQ003 and JQ201105), and the Innovation Research Program of China University of Petroleum (27R1104067A).

- Holmes T C, de Lacalle S, Su X, et al. Extensive neurite outgrowth and active synapse formation on self-assembling peptide scaffolds. *Proc Natl Acad Sci USA*, 2000, 97: 6728–6733
- Kisiday J, Jim M, Kurz B, et al. Self-assembling peptide hydrogel fosters chondrocyte extracellular matrix production and cell division: Implications for cartilage tissue repair. *Proc Natl Acad Sci USA*, 2002, 99: 9996–10001
- Silva G A, Czeisler C, Niece K L, et al. Selective differentiation of neural progenitor cells by high-epitope density nanofibers. *Science*, 2004, 303: 1352–1355
- Kretsinger J K, Haines L A, Ozbas B, et al. Cytocompatibility of self-assembled beta-hairpin peptide hydrogel surfaces. *Biomaterials*, 2005, 26: 5177–5186
- Beniash E, Hartgerink J D, Storrer H, et al. Self-assembling peptide amphiphile nanofiber matrices for cell entrapment. *Acta Biomater*, 2005, 1: 387–397
- Gelain F, Bottai D, Vescovi A, et al. Designer self-assembling peptide nanofiber scaffolds for adult mouse neural stem cell 3-dimensional cultures. *PLoS One*, 2006, 1: e119
- Nagai Y, Unsworth L D, Koutsopoulos S, et al. Slow release of molecules in self-assembling peptide nanofiber scaffold. *J Control Release*, 2006, 115: 18–25
- Jayawarna V, Ali M, Jowitt T A, et al. Nanostructured hydrogels for three-dimensional cell culture through self-assembly of fluorenyl-methoxycarbonyl-dipeptides. *Adv Mater*, 2006, 18: 611–614
- Haines-Butterick L, Rajagopal K, Branco M, et al. Controlling hydrogelation kinetics by peptide design for three-dimensional encapsulation and injectable delivery of cells. *Proc Natl Acad Sci USA*, 2007, 104: 7791–7796
- Jung J P, Nagaraj A K, Fox E K, et al. Co-assembling peptides as defined matrices for endothelial cells. *Biomaterials*, 2009, 30: 2400–2410
- Gelain F, Unsworth L D, Zhang S. Slow and sustained release of active cytokines from self-assembling peptide scaffolds. *J Control Release*, 2010, 145: 231–239
- Galler K M, Aulisa L, Regan K R, et al. Self-assembling multidomain peptide hydrogels: Designed susceptibility to enzymatic cleavage allows enhanced cell migration and spreading. *J Am Chem Soc*, 2010, 132: 3217–3223
- Williams R J, Hall T E, Glattauer V, et al. The *in vivo* performance of an enzyme-assisted self-assembled peptide/protein hydrogel. *Biomaterials*, 2011, 3: 5304–5310
- Bakota E L, Wang Y, Danesh F R, et al. Injectable multidomain peptide nanofiber hydrogel as a delivery agent for stem cell secretome. *Biomacromolecules*, 2011, 12: 1651–1657
- Bulut S, Erkal T S, Toksoz S, et al. Slow release and delivery of antisense oligonucleotide drug by self-assembled peptide amphiphile nanofibers. *Biomacromolecules*, 2011, 12: 3007–3014
- Hartgerink J D, Beniash E, Stupp S I. Self-assembly and mineralization of peptide-amphiphile nanofibers. *Science*, 2001, 294: 1684–1688
- Schneider J P, Pochan D J, Ozbas B, et al. Responsive hydrogels from the intramolecular folding and self-assembly of a designed peptide. *J Am Chem Soc*, 2002, 124: 15030–15037
- Hartgerink J D, Beniash E, Stupp S I. Peptide-amphiphile nanofibers: A versatile scaffold for the preparation of self-assembling materials. *Proc Natl Acad Sci USA*, 2002, 99: 5133–5138
- Rajagopal K, Lamm M S, Haines-Butterick L A, et al. Tuning the pH responsiveness of β -hairpin peptide folding, self-assembly, and hydrogel material formation. *Biomacromolecules*, 2009, 10: 2619–2625
- Zhang S, Holmes T, Lockshin C, et al. Spontaneous assembly of a self-complementary oligopeptide to form a stable macroscopic membrane. *Proc Natl Acad Sci USA*, 1993, 90: 3334–3338
- Ozbas B, Kretsinger J, Rajagopal K, et al. Salt-triggered peptide folding and consequent self-assembly into hydrogels with tunable modulus. *Macromolecules*, 2004, 37: 7331–7337
- Micklitsch C M, Knerr P J, Branco M C, et al. Zinc-triggered hydrogelation of a self-assembling β -hairpin peptide. *Angew Chem Int Ed*, 2011, 123: 1615–1617
- Pochan D J, Schneider J P, Kretsinger J, et al. Thermally reversible hydrogels via intramolecular folding and consequent self-assembly of a de novo designed peptide. *J Am Chem Soc*, 2003, 125: 11802–11803
- Haines L A, Rajagopal K, Ozbas B, et al. Light-activated hydrogel formation via the triggered folding and self-assembly of a designed peptide. *J Am Chem Soc*, 2005, 127: 17025–17029
- Toledano S, Williams R J, Jayawarna V, et al. Enzyme-triggered self-assembly of peptide hydrogels via reversed hydrolysis. *J Am Chem Soc*, 2006, 128: 1070–1071.
- Caplan M R, Schwartzfarb E M, Zhang S, et al. Control of self-

- assembling oligopeptide matrix formation through systematic variation of amino acid sequence. *Biomaterials*, 2002, 23: 219–227
- 27 Bowerman C J, Nilsson B L. A reductive trigger for peptide self-assembly and hydrogelation. *J Am Chem Soc*, 2010, 132: 9526–9527
 - 28 Jung J P, Jones J L, Cronier S A, et al. Modulating the mechanical properties of self-assembled peptide hydrogels via native chemical ligation. *Biomaterials*, 2008, 29: 2143–2151
 - 29 Xu H, Wang Y M, Ge X, et al. Twisted nanotubes formed from ultrashort amphiphilic peptide I₃K and their templating for the fabrication of silica nanotubes. *Chem Mater*, 2010, 22: 5165–5173
 - 30 Xu H, Wang J, Han S Y, et al. Hydrophobic-region-Induced transitions in self-assembled peptide nanostructures. *Langmuir*, 2009, 25: 4115–4123
 - 31 Wang J, Han S Y, Meng G, et al. Dynamic self-assembly of surfactant-like peptides A₆K and A₉K. *Soft Matter*, 2009, 5: 3870–3878
 - 32 Chen C X, Pan F, Zhang S Z, et al. Antibacterial activities of short designer peptide: A link between propensity for nanostructuring and capacity for membrane destabilization. *Biomacromolecules*, 2010, 11: 402–411
 - 33 Han S Y, Cao S S, Wang Y M, et al. Self-assembly of short peptide amphiphiles: The cooperative effect of hydrophobic interaction and hydrogen bonding. *Chem Eur J*, 2011, 17: 13095–13102
 - 34 Ellman G L. Tissue sulfhydryl groups. *Arch Biochem Biophys*, 1959, 82: 70–77
 - 35 Akaji K, Tatsumi T, Yoshida M, et al. Disulfide bond formation using the silyl chloride-sulfoxide system for the synthesis of a cystine peptide. *J Am Chem Soc*, 1992, 114: 4137–4143
 - 36 Schneider J P, Pochan D J, Ozbas B, et al. Responsive hydrogels from the intramolecular folding and self-assembly of a designed peptide. *J Am Chem Soc*, 2002, 124: 15030–15037
 - 37 Barth A, Zscherp C. What vibrations tell about proteins. *Q Rev Biophys*, 2002, 35: 369–430
 - 38 Yan H, Saiani A, Gough J E, et al. Thermoreversible protein hydrogel as cell scaffold. *Biomacromolecules*, 2006, 7: 2776–2782
 - 39 Krysmann M J, Castelletto V, Kelarakis A, et al. Self-assembly and hydrogelation of an amyloid peptide fragment. *Biochemistry*, 2008, 47: 4597

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Supporting Information

Figure S1 MALDI-TOF mass spectra of (a) Ac-I₃CGK-NH₂ and (b) Ac-I₃MGK-NH₂.

Figure S2 HPLC profiles of (a) Ac-I₃CGK-NH₂ and (b) Ac-I₃MGK-NH₂.

Figure S3 The calibration curve of UV absorbance at 412 nm as a function of H-Cys-OH·HCl concentration. The linearly dependent coefficient was 0.99989.

Figure S4 TEM characterization of the self-assembled structures from the oxidized Ac-I₃CGK-NH₂ dimers.

Figure S5 AFM characterization (5 μm×5 μm) of protofibrils formed by Ac-I₃CGK-NH₂ in the first few hours after dissolution.

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